

PERFORMANCE OF K-NEAREST NEIGHBOR BASED CLASSIFIER FOR CLASSIFICATION OF CARDIOTOCOGRAMS

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Abstract: Fetal heart rate (FHR) and uterine contractions (UC) are simultaneously recorded by Cardiotocography (CTG). The CTG, which is one of the most common diagnostic techniques used to evaluate maternal and fetal well-being during pregnancy and before delivery. By observing the Cardiotocography trace patterns doctors can understand the state of the fetus. There are several signal processing and computer programming based techniques for interpreting typical Cardiotocography data. Even few decades after the introduction of cardiotocography into clinical practice, the predictive capacity of these methods remains controversial and still inaccurate. In this research work I propose an integrated methodology for CTG analysis and classification. A novel set of features, derived from the time and frequency domains, is used to feed the new tool for pattern classification, named K-Nearest neighbor. We used Accuracy, Specificity, NPV, Precision, Recall and ROC as the metric to evaluate the performance. The arrived results prove that, even though the traditional clustering methods can identify the Normal CTG patterns, they were incapable of Suspicious and Pathologic patterns. It was found that, the K-Nearest neighbor based classifier was capable of identifying Normal, Suspicious and Pathologic condition, from the nature of CTG data.

Keywords—

CTG, Datamining, Classification, fetal heart rate, uterine contractions and K-Nearest neighbor

I. INTRODUCTION

Datamining refers to a collection of techniques that provide the necessary actions to retrieve and gather knowledge from an exhaustive collection of data and facts. Data is available in enormous magnitude, but the knowledge that can be inferred from the data is still negligible. Datamining concepts are focused on discovering knowledge, predicting trends and eradicating superfluous data. Discovering knowledge in medical systems and healthcare scenarios is a herculean effort critical task. Knowledge discovery describes the process of automatically searching large volumes of data for patterns that can

be considered additional knowledge about the data. The knowledge obtained through the process may become additional data that can be used for further manipulation and discovery. Application of data mining concepts to the medical arena has undoubtedly made remarkable strides in the sphere of medical research and clinical practices saving time, money and life. Clinical data mining is the application of data mining techniques using clinical data. Clinical Data-Mining (CDM) involves the conceptualization, extraction, analysis, and interpretation of available clinical data for practical knowledge-building, clinical decision-making and practitioner reflection. The main objective of clinical data mining is to haul new and previously unknown clinical solutions and patterns to aid the clinicians in diagnosis, prognosis and therapy. Moreover application of softwares solution to store patient records in electronic form is expected to make mining knowledge from clinical data less stressful.

A. Cardiotocography (CTG)

Since the 1960's, obstetricians are using the Cardiotocography, an electronic method for recording (graphy) the fetal heartbeat (cardio) and uterine contractions (toco) during pregnancy, by means of a Cardiotocograph or electronic fetal monitor (EFM). Fig. 1 illustrates a typical Cardiotocogram (CTG).

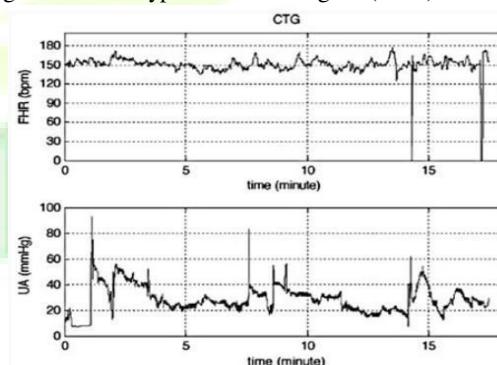


Figure 1. Atypical CTG[4]

The continuous monitoring by using CTG requires qualitative and quantitative interpretations of several parameters described as follows [3]:

Uterine activity (contractions):

- Frequency: Number of contraction in a standard interval.
- Duration: The amount of time from the start of a contraction to the end of the same contraction.
- Intensity: A measure of how strong a contraction is.
- Resting tone: A measure of how relaxed the uterus is between contractions.
- Interval: The amount of time between the end of one contraction to the beginning of the next contraction.

Uterine activity may be defined as:

- Normal - less than or equal to 5 contractions in 10 minutes, averaged over a 30-minute window.
- Tachysystole - more than 5 contractions in 10 minutes, averaged over a 30-minute window.

Baseline fetal heart rate (FHR), which is determined by approximating the mean FHR rounded to increments of five beats per minute during a 10-minute window, excluding accelerations and decelerations and periods of marked FHR variability.

- Baseline FHR less than 110 beats per minute and symptoms are termed Bradycardia.
- Baseline FHR greater than 160 beats per minute and symptoms are termed tachycardia.

Baseline FHR variability, which is determined in a 10-minute window, excluding accelerations and decelerations. Baseline FHR variability is defined as fluctuations in the baseline FHR that are irregular in amplitude and frequency. These fluctuations are visually quantified as the amplitude of the peak-to-trough in bpm (beat per minute).

- Absent
- Minimal
- Moderate
- Marked

Presence of accelerations: Visually apparent abrupt increase in FHR. An abrupt increase is an increase from a non-stationary baseline to the peak in less than or equal to 30 seconds (to be considered as acceleration, the peak must be greater than or equal to 15 bpm).

Periodic or episodic decelerations

- Periodic: Refers to decelerations that are associated with contractions.

- Episodic: Refers to those not associated with contractions

There are four types of decelerations:

- Early deceleration: It is related to a gradual decrease in the FHR with an onset of deceleration to anadir (more than 30 seconds) where the nadir occurs within the peak of a contraction.
- Late deceleration: It is related to a gradual decrease in the FHR with an onset of deceleration to anadir (more than 30 seconds).
- Variable deceleration: It is related to an abrupt decrease in the FHR (more than 15 bpm) that was measured from the most recently baseline where from the deceleration's onset to nadir is less than 30 seconds and the deceleration lasts (more than 15 seconds).
- Prolonged deceleration: It is present when there is a visually apparent decrease in FHR from the baseline that is greater than or equal to 15 bpm, lasting greater than or equal to 2 minutes, but less than 10 minutes. A deceleration that lasts greater than or equal to 10 minutes is a baseline change. Changes or trends of FHR patterns over time.
- Category I (Normal): Baseline rate 110-160 bpm, Moderate variability, Absence of late, or variable decelerations, and early decelerations and accelerations may or may not be present.
- Category II (Indeterminate): Tracing is not predictive of abnormal fetal acid-base status, but evaluation and continued surveillance and reevaluations are indicated.
- Category III (Abnormal): Absence of baseline variability with recurrent late or variable decelerations or Bradycardia; or sinusoidal fetal heart rate.

II. RELATED WORK

The International Federation of Obstetrics and Gynaecology (FIGO) guidelines [5] were introduced as an attempt to standardize the use of electronic monitoring of FHR. The first work of automatic CTG analysis following FIGO guidelines consists in describing and extracting the CTG morphological features [6]. Bernades [7] developed SisPorto, a system for automatic analysis of CTG tracings, based on an improvement of the morphological feature extraction introduced in [6].

Artificial Neural Networks (ANNs) were used as a classifier [8] to detect FHR acceleration and decelerations and to estimate the FHR baseline and variability. ANNs were used to classify deceleration patterns into episodic and periodic decelerations [9] according to FIGO guidelines and based on the relationship between the parameters of

the deceleration and the associated uterine contraction. ANNs with Radial Basis Functions (RBF) and Multi Layer Perceptrons (MLP) were the best performing classifiers.

Support Vector Machines (SVM) have been used for FHR signal analysis. Georgoulas et al. [10] used discrete wavelet transformation to extract scale-dependent features of the FHR signal and SVM for their classification. Georgoulas et al. [11] used SVM with RBF and polynomial kernel to identify fetal and neonatal compromise, namely metabolic acidosis [12]. The RBF kernel machines outperformed the polynomial machines and both of them outperformed the conventional methods of k-nearest neighbor (k-NN), linear and quadratic discriminant classifiers.

Chudáček et al. [13] used SVM, naïve Bayes, and a decision tree (C4.5 algorithm) with a polynomial kernel to analyze FHR signals based on linear features (e.g. Description of the FHR baseline using mean) and non-linear features (e.g. Fractal dimension of waveform). They used three FSm methods: Principal Component Analysis, Information Gain, and Group of Adaptive Models Evolution (GAME).

Krupa et al. [14] proposed a new method for FHRs signal analysis based on Empirical Mode Decomposition (EMD) of feature extraction and SVM with RBF for classification of FHR recordings.

Georgoulas et al. [15] proposed a FS method base don bPSO (binary Particle Swarm Optimization) for FHR signal analysis using SVM and k-NN.

Hybrid methods have been also considered for automated FHR signal analysis. Fontenla-Romero et al. [16] proposed several approaches for the recognition of acceleration and deceleration patterns in FHR signals, including rule-based approach, ANNs, and a neuro-fuzzy approach.

III. MOTIVATION AND JUSTIFICATION

Cardiotocography (CTG), consisting of fetal heart rate (FHR) and tocographic (TOCO) measurements, is used to evaluate fetal well-being during the delivery. Since 1970, many researchers have worked different mining methods to help the doctors that interpret the CTG trace pattern from the field of signal processing and computer programming [18]. With the help of CTG trace pattern analysis the doctors with interpretations in order to reach a satisfactory level of reliability. So, they act as a decision support system in obstetrics. For everyday practice, none of them has been adapted worldwide. Baseline estimation in computer analysis of cardiotocographs, which is currently no consensus on the best methodology. More than 30 years after the introduction of antepartum cardiotocography into clinical practice, the predictive capacity of the method remains controversial. In a review of lots of articles published on this subject, it was found that its reported sensitivity varies between 2 and 100%, and its specificity between 37 and 100% [19]. So, in this

work, we are going to evaluate K-Nearest neighbor algorithms for clustering CTG data.

IV. MATERIAL AND METHODOLOGY

A. DATASET DESCRIPTION

The Cardiotocography dataset used in this study is publicly available at The Data Mining Repository of University of California Irvine (UCI). By using 21 given attributes data can be classified according to FHR pattern class or fetal state class code. In this study, fetal state class code is used as target attribute instead of FHR pattern class code and each sample is classified

into one of three groups Normal, Suspicious or Pathologic. The dataset includes a total of 216 samples of which is 1655 normal, 295 suspicious and 176 pathologic samples which indicate the existing of fetal distress.

Attribute information is given as:

- LB—FHRbaseline (beats per minute)
- AC—# of accelerations per second
- FM—# of fetal movements per second
- UC—# of uterine contractions per second
- DL—# of light decelerations per second
- DS—# of severe decelerations per second
- DP—# of prolonged decelerations per second
- ASTV—percentage of time with abnormal short term variability
- MSTV—mean value of short term variability
- ALTV—percentage of time with abnormal long term variability
- MLTV—mean value of long term variability
- Width—width of histogram
- Min—minimum of histogram
- Max—Maximum of histogram
- Nmax—# of histogram peaks
- Zeros—# of histogram zeros
- Mode—histogram mode
- Mean—histogram mean
- Median—histogram median
- Variance—histogram variance
- Tendency—histogram tendency
- CLASS—
- FHRpatternclasscode(1 to 10)—class code (N = normal; S = suspect; P = pathologic)

B. CLASSIFICATION

Classification process may be applied in different areas of research and practice, e.g., farms, military, medicine, Earth resources sensing. The classical classification techniques use statistical approach, which typically assumes the normal multidimensional distribution of probability in the experimental dataset. Data classification may be supervised and unsupervised. The supervised classification method requires the presence of training data set typically defined by the expert or the teacher. Each class of objects is characterised by the basic statistical parameters

(mean values vector, covariance matrix), which are values vector, covariance matrix), which are recomputed from the training set. These parameters guide the discrimination process. The Bayesian classifiers are typical representatives (Bayes classifier, Fisher, Wald sequential).

The unsupervised classification is also known as classification without the teacher. This classification uses, in most cases, the methods of cluster analysis. The device that performs the function of classification is called classifier. The classifier is the system containing several input paths that are transported with signals carrying information about the objects. The system generates information about the competence of objects into a particular class on the output.

C. THE MEDICAL BACKGROUND OF CARDIOTOCOGRAPHY (CTG)

Cardiotocography is a medical test conducted during pregnancy that records fetal heart rate (FHR) and uterine contractions. Either internal or external methods the tests may be conducted. During the internal testing, the uterus is placed by a catheter after a specific amount of dilation has taken place. The external tests, a pair of sensory nodes are affixed to the mother's stomach. The CTG trace generally shows two lines. The fetal heart rate is recorded by the upper line in beats per minute and the uterine contractions are recorded by the lower line from the TOCO.

Baseline Heart Rate

The baseline heart rate helps to evaluate the health functioning of the cardiovascular system. The baseline fetal heart rate is determined by approximating the mean FHR rounded to increments of 5 beats per minute (bpm) during a 10-minute window, excluding accelerations and decelerations and periods of marked FHR variability (greater than 25 bpm). Abnormal baseline is termed bradycardia and tachycardia. The fluctuations are visually quantified as the amplitude of the peak-to-trough in bpm. Using this definition, the baseline FHR variability is categorized by the quantities amplitude as:

Absent-undetectable

Minimal-
greater than undetectable, but less than or equal to 5 bpm

Moderate-6 bpm-25 bpm
Marked-
greater than 25 bpm

Bradycardia:

It is the resting heart rate of under 60 beats per minute, though it is seldom symptomatic until the rate drops below 50 beats/min. It may cause cardiac arrest in some patients. Tachycardia: It typically refers

to a heart rate that exceeds the normal range for a resting heart rate (heart rate in an inactive or sleeping individual). Depending on the speed and type of rhythm, it can be dangerous.

Type 1 (early)

This occurs during the peak of the uterine contraction. The FHR with onset early in the contraction and return to baseline at the end of the contraction will be uniform, repetitive and periodic slowing. The reasons behind this maybe fetal head compression, cord compression or early hypoxia. This occurs in first and second stage labor with decent of the head [21]. This is synchronous with uterine contraction.

Type 2 (late)

This occurs after the peak of the uterine contraction. The FHR with onset mid to end of the contraction nadir more than 20 seconds after the peak of the contraction and ending after the contraction will also be uniform, repetitive and slowing. If the lag time is high seriousness is also high. This is also synchronous with uterine contraction. Mx: afetal pH measurement is mandatory [21].

Type 3 (variable)

This is variable, repetitive, and periodic slowing of FHR with rapid onset and recovery. Variable and isolated timerelationships with contraction cycles may occur. Deceleration patterns in timing and shape resemble other types in some cases. If they occur consistently, there is a chance of fetal hypoxia. This is unrelated to uterine contractions. Mx: check fetal pH if the pattern persists after turning the patient onto the side (or if other adverse features are present) [21].

A. D.K-Nearest neighbor

The k-nearest neighbors are an example of a classification method with the independence of the parameters. The method can be classified as by the point of implication as simple, but efficient in many datasets [11]. The k-NN algorithm is defined by three terms (S, k, T) where S represents a resemblance measure which links to a pair of data in an appropriate N -dimensional space at (real or integer) number, k represents the number of nearest data that are retrained to carry out the classification and T represents the vector of M training data applied by the classifier to actually carry out the classification [12]. k-NN uses distance metrics usually Euclidean distance to perform the similarity measure formulated by

$$d_E = \sum_{i=1}^N \sqrt{x_i^2 - y_i^2}$$

If it is a data sample, which classification implemented a nd its k nearest neighbor turn up, then this makes a neighborhood of. When using the method to classify the data sample in the neighborhood about, the distance is whether considered or not. Of course, to use k-NN choosing the right value for k is critical; due to the rate of success of classification directly appertains to this value. The k-NN method can pass for biased by k. It is possible to choose the k-value in so many different ways. Of course, the smooth and efficient one is applying the algorithm several times changing the value of k to get the highest accuracy. To decrease the dependency level of choice of k for k-NN method, Wang [13] recommended checking multiples sets of nearest neighbors instead of one set of nearest neighbors.

V. EXPERIMENTATION RESULT

A. PERFORMANCE EVALUATION

This is a measurement tool to calculate the performance

$$\text{Accuracy} = \left[\frac{TP + TN}{TP + TN + FP + FN} \right]$$

$$\text{Sensitivity} = \left[\frac{TP}{TP + FN} \right]$$

$$\text{Specificity} = \left[\frac{TN}{TN + FP} \right]$$

$$\text{Positive Predictive Value: } PPV = \left[\frac{TP}{TP + FP} \right]$$

$$\text{Negative Predictive Value: } NPV = \left[\frac{TN}{TN + FN} \right]$$

$$ROC = \frac{sensitivity + specificity}{2}$$

Where

- The *false negative rate* (*FN*) is the proportion of positive cases that were incorrectly classified as negative.
- The *accuracy* (*AC*) is the proportion of the total number of predictions that were correct.
- The *Sensitivity* or *Recall* is the proportion of actual positive cases which are correctly identified.
- The *Specificity* is the proportion of actual negative cases which are correctly identified.
- The *Positive Predictive Value* or *Precision* is the proportion of positive cases that were correctly identified.
- The *Negative Predictive Value* is the proportion of negative cases that were correctly identified.

TABLE I: PERFORMANCE ANALYSIS OF K-NEAREST NEIGHBOR USING CROSS VALIDATION

Performance	K-Nearest N
Accuracy	97.4230
Sensitivity	96.3320
Specificity	96.6219
PPV	94.7793
NPV	97.5064
ROC	91.9874

VI. CONCLUSION

This work has evaluated the performance of the K-Nearest neighbour Algorithm with respect to confusion matrix and accuracy. According to that K-Nearest neighbour Algorithm based classification approach provided significantly poor performance. It was found that the K-Nearest neighbour Algorithm classifier was capable of identifying Normal, Suspicious and Pathologic condition, from the nature of CTG data with comparatively poor accuracy. If we consider only the precision as a metric, then arrived results prove that, even though the machine learning based methods can distinguish the Normal CTG

- The recall or true positive rate (*TP*) is the proportion of positive cases that were correctly identified
 - The false positive rate (*FP*) is the proportion of negative cases that were incorrectly classified as positive
 - The true negative rate (*TN*) is defined as the proportion of negative cases that were classified correctly
- B. patterns from the Suspicious and Pathologic patterns with respect to precision and pathologic, but, they were incapable of distinguishing Suspicious. That is why we are getting comparatively poor average performance while classifying suspicious records with respect to precision. It is a major weakness of the algorithms which should be overcome in future design. One may address the way to improve the system forgetting proper results with different
- C. classes of CTG patterns. One may consider machine learning based method to design the CTG data classification system. Future works may address hybrid models using statistical and machine learning technique for improved classification accuracy.
- D.
- E. In future work, we plan to collaborate with obstetric clinicians and physicians in order to assess the computational results.

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